

Why the ISMNI and the Utah paradigm? Their role in skeletal and extraskeletal disorders

H.M. Frost

Department of Orthopaedic Surgery, Southern Colorado Clinic, USA

Abstract

Besides bringing problems, aging can let the mind's eye see more clearly than before, and it can let us express ourselves better. As age, experience and common sense examine today's skeletal medicine and surgery two questions keep popping up: *A) How did we fail?; B) How to make it better?* The Utah paradigm of skeletal physiology and the seminal ISMNI offer some answers, but exploiting them faces problems. Problem #1: By 1960 all clinicians and physiologists "knew" (as the ancients "knew" this world is flat) that effector cells controlled solely by nonmechanical agents explain all skeletal physiology and disorders ("effector cells" include osteoblasts, osteoclasts, chondroblasts and fibro-blasts). Or, *nonmechanical agents* → *cell level* → *organ and intact subject*. Adding later-discovered information to that 1960 view led to the Utah paradigm, which reveals the formerly hidden tissue-level "dimension" of skeletal physiology. It builds on this idea: (*mechanical + nonmechanical agents*) → (*tissue level + cell level*) → *organ and intact subject*. The paradigm assigns great influence of neuromuscular physiology and physical activities on skeletal architecture, strength and mechanical competence. It also exposes flaws in many older views so controversies arise. Problem #2: The Utah paradigm and Wegner's concept of plate tectonics in geology seem alike in that each is valid but came before its time, so others fought it. They differ in this: The fight about Wegner's idea is over, but for the Utah paradigm and the ISMNI it just began. Hence more controversies. Nevertheless: A growing minority realizes that paradigm provides a far better base to build on than its antecedents, and since it keeps evolving as more evidence comes in it could endure for some decades. Yet very few realize this: *It and the ISMNI have important implications for fields besides biomechanics and orthopaedics*¹⁸. Examples include anatomy, cardiovascular disease, dentistry, endocrinology, family medicine, gastroenterology, general surgery, genetics, gerontology, gynecology, maxillofacial surgery, neurology, neurosurgery, nutrition, ophthalmology, pathology, pediatrics, physical medicine and rehabilitation, plastic surgery, radiology, rheumatology, space and sports medicine, and urology. Quite a list! For the italicized questions above this article offers answers, of which its conclusion distills an essence.

Keywords: Physiology, Bone, Joint, Tendon, Biomechanics, Skeleton, Utah Paradigm

Introduction

The multidisciplinary Utah paradigm and the ISMNI have implications for the future research and management of many clinical problems, and for the pharmaceutical industry. This article summarizes some of the Utah paradigm's features to provide some sense of it and of the scope of the ISMNI that provides its second forum. The first forum: The University of Utah's Hard Tissue Workshops³¹.

As for that paradigm's origins, before 1950 physiologists realized renal function depends on the kidney's many kinds

of cells and the functions of tissue-level nephrons made with those cells. Nephrons provide functions no single kind of cell can provide, but they are essential for our health. The same idea applies to the lung, gut, liver and endocrine organs, as examples only.

However ideas about skeletal physiology took a different path. Bone can illustrate it. By 1900 it was known that osteoblasts make bone and osteoclasts resorb it³⁵, but no skeletal "nephron equivalent" functions were recognized before 1964. Ergo, by 1960 everybody "knew" bone's effector cells (osteoblasts and osteoclasts) wholly determine bone health and disorders under the sole control of non-mechanical agents^{1,39,47}.

That idea was extrapolated to collagenous tissue and cartilaginous organs too^{1,2,34}, for which fibroblasts and chondroblasts respectively provide the effector cells²⁷.

Corresponding author: Harold M. Frost, Department of Orthopaedic Surgery, Southern Colorado Clinic, PO Box 9000, Pueblo, CO 81008-9000, USA.

Accepted 15 February 2000

organs satisfy Proposition #1. Many nonmechanical agents could modulate but not replace that function, in part by changing the genetically-determined strain thresholds^{21,28-30,37,43,46}.

In the mechanostat hypothesis the skeleton's nephron equivalents would be like a car's steering, brakes and accelerator, and effector cells would be like its wheels. Voluntary mechanical usage would be like its driver. Implication: As studying only the wheels could not explain why a car drove to Milan instead of Rome, in the paradigm's view studying only effector cells would seldom explain why an osteoporosis, arthrosis, some healing problem or a spontaneous tendon rupture occurred**.

The post-1950 studies of effector-cell roles in repair processes [3,4] overlooked the four essential tissue-level stages of healing in all skeletal tissues ("essential" because if any stage fails so does healing)^{10,32,48**}. A) At first some kind of soft callus forms. B) Then a remodeling mechanism replaces it with the mature kind of tissue, C) while modeling reshapes and sizes it to provide normal strength. D) A concurrent RAP accelerates "A-C". Strains, presumably in the adapted and mild overload windows¹⁵, help to guide and potentiate "A-C" in time and space. The whole healing process would make injured organs satisfy Proposition #1 again. Impairments of those four stages cause several kinds of "biologic failures" of healing (ones not due to treatment errors)³².

Nota bene: In 2000 AD many physiologists and clinicians might find some of the above information and ideas strange, even radical. Nevertheless I am certain they are valid.

Discussion

1) On the roles of hormones, other humoral and non-mechanical agents, genetics and cytokines.

Past basic research focused so much on how such factors affect the skeleton's effector cells (the skeleton's "wheels")^{2-4,7,34} that proven knowledge (as opposed to opinions) about their effects on the skeleton's nephron-equivalent functions remains very sketchy. Yet those functions help to determine the phenotypes of bones, joints, tendons and ligaments, as well as our body height and limb lengths and alignments**. In my view explaining such things solely in terms of effector cell effects would be like trying to explain why a car drove to Milan instead of Rome by only studying its wheels. How agents affect the skeleton's effector cells in current cell, tissue and organ-culture systems seldom predict correctly how such agents affect skeletons in vivo. Why? As Michael Parfitt also noted⁴⁰, bone's nephron equivalents do not function and respond normally in present in vitro systems^{9,19}. That means one should study them in vivo. WSS Jee led the way in showing how²⁸⁻³¹.

A few implications. The above physiology has too many implications for future research and clinical management to list here. A few examples: The cell and molecular biology on which all the skeleton's nephron-equivalent functions

depend need systematic study; we need normal standards for the muscle/skeletal-organ/strength relationships⁸; we need more reliable noninvasive indicators of whole-organ strength⁸; neurophysiologic effects on skeletal modeling, remodeling and maintenance need extensive study; space and sports medicine, pathology, rheumatology and hard and soft tissue healing studies^{32,48} need to account for the Utah paradigm's insights; current schemes for diagnosing and classifying osteoporoses, arthroses, healing problems and developmental disorders need revision and/or supplementation²⁵; the signalling mechanisms that help to control nephron-equivalent functions need more study^{26,36}; and the roles of collagenous tissue physiology and different collagen Types in problems in the medical specialties mentioned in the Abstract need systematic study¹⁸.

2) Some special features of bone and bones^{9,11,12}.

Separate formation and resorption drifts provide bone modeling²⁷. They determine the cross sectional size and shape and the longitudinal shape of bones and trabeculae, and thus their strength. Mechanically-controlled bone modeling works best during growth³⁷. It becomes inefficient in adult cortical bone but it can affect trabeculae throughout life. A mediator mechanism in bone marrow helps to control modeling and remodeling of bone next to it^{20**}. It can cause disuse-mode remodeling of bone next to marrow, and it causes all adult-acquired osteopenias on earth and in orbit**. Chronic muscle weakness for any reason usually causes a "physiologic osteopenia" in which bones satisfy Proposition #1, since only injuries would cause fractures^{22**}. Yet some modeling and remodeling disorders can cause a "true osteoporosis" in which voluntary activities cause fractures, so Proposition #1 is not satisfied^{22**}. Growing cartilage layers at the ends of most bones (growth plates and articular cartilage) determine their length^{9,28}. Partly under biomechanical control, another nephron-equivalent mechanism called endochondral ossification replaces the added cartilage with spongiosa^{16,17,27}.

3) Some special features of fascia, ligament, tendon and collagenous tissue^{9,24}.

When this tissue's strains exceed its modeling threshold it adds collagen to thicken and strengthen the affected organ without changing its length. In collagenous tissues this mechanically-controlled diametric modeling ability lasts for life^{14**}. It makes the strength of tendons exactly match the muscle forces on them**. When strains stay below this tissue's "remodeling threshold" cellular mechanisms reduce its collagen content and the affected structure becomes thinner and weaker. Unlike healthy bone, under constant tension loads collagenous tissue also can stretch or "creep" irreversibly (not the same thing as viscoelastic deformation)**. A "creep compensation" mechanism can prevent or correct limited amounts of it^{14**}. Excessive creep compensation causes joint contractures, and contractures in

Dupuytren's and Peyronie's diseases**. Failure of that mechanism can cause lax joints, for example in rheumatoid arthritis and Ehler-Danlos syndrome**. Collagenous tissues can repair limited amounts of microdamage in their collagen, and failure to do it causes, among other things, spontaneous tendon ruptures and, in the vertebral annulus, many spinal disc problems**.

Normally this tissue's modeling, creep compensation and microdamage repair mechanisms make collagenous organs satisfy Proposition #1**. Problems with those mechanisms cause or help to cause all spontaneous ruptures of tendons, ligaments and muscles. A growing layer of cartilage at the bony attachments of ligament, tendon and fascia helps to lengthen them in childhood, when ligaments and fascia can also increase in length ("grow") by the creep mechanism**.

Nota bene: Interstitial collagen, and/or collagenous sheaths, membranes, capsules, adventitia and fascia hold all soft tissue organs together. Accordingly collagen problems can cause or help to cause many extraskelatal disorders. A few examples include some varices, aneurysms, hernias, strictures and stenoses; myopia and hyperopia; hepatic cirrhosis; pericardial stenosis and intestinal obstructions from adhesions; arthrogryposis; scleroderma; and sagging skin and breasts with aging. Hence the implications of this paradigm for many medical specialties listed in this article's Abstract.

4) Some special features of joints and cartilage^{13,23}.

During growth mechanically-controlled chondral modeling affects the size and shape of joints, the thickness of articular cartilage, and the congruence or "fit" of opposed joint surfaces. It makes growing joints large enough and strong enough to satisfy Proposition #1**. Cartilage strains above a threshold range can turn this mechanically-controlled modeling on; otherwise it stays off**. Normal chondral modeling nearly stops at and after skeletal maturity, so adult joints must depend largely on maintenance functions to endure their mechanical usage [9]. Hyaline and fibrocartilage can repair limited amounts of microdamage in their collagen, and inadequate repair of it in articular cartilage is the "final cause" of most arthroses and of degenerated menisci in the knee and temporomandibular joints^{23**}. These tissues too can creep irreversibly and very slowly (also called "plastic flow", and not the same thing as viscoelastic deformation)**. Presumably they too have mechanisms that can prevent or correct limited amounts of creep²³. In combination, Chondral Modeling, Maintenance and Creep Compensation (CMMCC) make normal joints satisfy Proposition #1**; otherwise an arthrosis develops. Disorders of those mechanisms also cause or help to cause skeletal disorders like Marfan's syndrome, Morquio's disease, Blount's disease, achondroplasia, Madelung's deformity and congenital hip dysplasia**, which are also some "first causes" of arthroses**. Examples of other first causes include chondrocalcinosis, rheumatoid disease, pyarthroses and overloads due to joint malalignments and trauma³⁴.

Nota bene: CMMCC disorders can also cause or help to cause extraskelatal disorders of the ear and nasal cartilages, larynx, trachea and bronchia**.

5) Some recent history.

By 1990 the Utah paradigm suggested this: Neuromuscular function and physiology strongly influence, and may even dominate, control of the biologic mechanisms that determine the postnatal architecture and strength of load-bearing bones, joints, fascia, ligaments and tendons. In 1990 most people thought that idea was too radical to deserve testing, yet by 1999 both live-animal and human studies strongly supported it^{25,28-30,43,44}. I and some colleagues (JL Ferretti, WSS Jee, H Schiessl, E Schönau) are now certain that idea is valid. We understand and respect the doubts of others, but those studies clearly show the idea needs serious consideration. Only help from many people and disciplines can test it further, and we invite and welcome that.

The above material helps to explain the Utah paradigm's status in skeletal science, medicine and surgery today, when most people still view it as a "new kid on the block" and wait for proof they could accept of its worth. The ISMNI aims to explore and find how to exploit the above physiology. Neoplasia excepted, the broad domain of the Utah paradigm and the ISMNI includes most skeletal disorders as well as many disorders of soft tissue organs¹⁸.

Conclusion

As for the Abstract's two italicized questions: A) We overlooked the tissue-level skeleton's rich, golden Dorado; B) So, mine it!

References

1. Aegerter E, Kirkpatrick JA. Orthopaedic Diseases. WB Saunders Co, Philadelphia, 1975.
2. Albright JA, Brand RA. The Scientific Basis of Orthopaedics (2nd ed)(Eds) Appleton and Lange, Norwalk, 1987.
3. Barnes GL, Kostenuik PJ, Gerstenfeld LC, Einhorn TA. Growth factor regulation of fracture repair. J Bone Min Res 1999; 14:1805-1815.
4. Bilezikian JP, Raisz LG, Rodan GA. Principles of Bone Biology. Academic Press, Orlando, FL, 1996.
5. Burr DB, Forwood MR, Fyrhie DP, Martin RB, Schaffler MB, Turner CH. Bone microdamage and skeletal fragility in osteoporotic and stress fractures. J Bone Miner Res 1997; 12:6-15.
6. Burr DB. Muscle strength, bone mass, and age-related bone loss. J Bone Miner Res 1997; 12:1547-1551.
7. Currey JD. The Mechanical Adaptations of Bones. Princeton University Press, Princeton, 1984.
8. Ferretti JL, Frost HM, Schiessl H. On new opportunities for absorptiometry. J Clin Densitom 1998; 1:41-53.

9. Frost HM. Intermediary Organization of the Skeleton, Vols I,II. CRC Press, Boca Raton, 1986.
10. Frost HM. The biology of fracture healing. Clin Orthop Rel Res. Part I:248:283-293; Part II:248:294-309, 1989.
11. Frost HM. Structural adaptations to mechanical usage (SATMU):1. Redefining Wolff's Law: The bone modeling problem. Anat Rec 1990; 226:403-413.
12. Frost HM. Structural adaptations to mechanical usage (SATMU):2. Redefining Wolff's Law: The bone remodeling problem. Anat Rec 1990; 226:414-422.
13. Frost HM. Structural adaptations to mechanical usage (SATMU):3. The hyaline cartilage modeling problem. Anat Rec 1990; 226:423-432.
14. Frost HM. Structural adaptations to mechanical usage (SATMU):4. Mechanical influences on fibrous tissues. Anat Rec 1990; 226:433-439.
15. Frost HM. Perspectives: Bone's mechanical usage windows. Bone and Min 1992; 19:257-271.
16. Frost HM, Jee WSS. Perspectives: A vital biomechanical model of the endochondral ossification mechanism. Anat Rec 1994; 240:435-446.
17. Frost HM, Jee WSS. Perspectives: Applications of a biomechanical model of the endochondral ossification mechanism. Anat Rec 1994; 240:447-455.
18. Frost HM. Introduction To A New Skeletal Physiology. Vols I, II. The Pajaro Group, Inc., Pueblo, Colorado, 1995.
19. Frost HM. Perspectives: A proposed general model of the mechanostat (suggestions from a new paradigm). Anat Rec 1996; 244:139-147.
20. Frost HM. On rho, a marrow mediator and estrogen: Their roles in bone strength and "mass" in human females, osteopenias and osteoporoses (insights from a new paradigm). J Bone Miner Metab 1998; 16:113-123.
21. Frost HM. From Wolff's Law to the Mechanostat: A New "Face" of Physiology. J Orthopaedic Science 1998; 3:282-286.
22. Frost HM. Osteoporoses: New Concepts and Some Implications for Future Diagnosis, Treatment and Research (based on insights from the Utah paradigm). Ernst Schering Research Foundation AG, Berlin, pp 7-57, 1998.
23. Frost HM. Joint Anatomy, Design and Arthroses: Insights of the Utah Paradigm. Anat Rec 1999; 255:162-174.
24. Frost HM. The Utah paradigm of skeletal physiology: An overview of its insights for bone, cartilage and collagenous tissue organs. J Bone Min Metab (in press), 2000.
25. Frost HM, Jee WSS. Osteoporosis at a cross roads: Quo Vadis? J Bone Miner Res (in press), 2000.
26. Garcia AM, Frank EH, Grimshaw PE, Grodzinsky AJ. Contributions of fluid convection and electrical migration to transport in cartilage: Relevance to loading. Arch Biochem Biophys 1996; 333:317-325.
27. Jee WSS. The skeletal tissues. In: Cell and Tissue Biology. A Textbook of Histology. L Weiss (Ed). Urban and Schwarzenberg, Baltimore 1989:211-259.
28. Jee WSS. The anabolic agents and the mechanostat. In: Advances in Osteoporosis. Vol I. GP Lyritis (Ed). Hylonome Editions, Athens, Greece 1998:37-52.
29. Jee WSS, Zhou H, Yao W, Cui L, Ma YF. The interaction of mechanical loading and bone anabolic agents. In: Osteoporosis Update 1999. Proceedings, Third International Congress on Osteoporosis, 31 March - 3 April, Xi'an, P.R. China, 1999:78-83.
30. Jee WSS. The interactions of muscles and skeletal tissue. In: Musculoskeletal Interactions, Vol II. GP Lyritis (Ed). Hylonome Editions, Athens 1999:35-46.
31. Since 1965 WSS Jee, Professor of Anatomy at the University of Utah School of Medicine, organized uniquely seminal, multidisciplinary Hard Tissue Workshops. Sponsored by the University of Utah, worldwide they influenced how we think about and study skeletal physiology and disease more than any other meetings in this century. The Utah paradigm had its genesis there (hence its name), aided by input from numerous international authorities in many fields of skeletal science, medicine, surgery and pathology.
32. Jensen OT. The Sinus Bone Graft (Ed). Quintessence Publishing Co, Carol Stream, IL, 1998.
33. Kannus P, Sievanen H, Vuori L. Physical loading, exercise and bone. Bone 1996; 18 (Suppl 1):1-3.
34. Kippel JH, Dieppe PA. Rheumatology (Eds). Mosby-Year Book, Inc. 1994.
35. Lewis FT. Stohr's Histology (Ed). (6th U.S. ed) P Blakiston's Son and Co, Philadelphia, 1906.
36. Marotti G. The structure of bone tissues and the cellular control of their deposition. Ital J Anat Embryol 1996; 101:25-79.
37. Martin RB, Burr DB, Sharkey NA. Skeletal Tissue Mechanics. Springer-Verlag, New York, 1998.
38. Martin RB. Towards a unifying theory of bone remodeling. Bone 2000; 26:1-6.
39. McLean FC, Urist MR. Bone (2nd ed). University of Chicago Press, Chicago, 1961.
40. Parfitt AM. Problems in the application of in vitro systems to the study of human bone remodeling. Calcif Tiss Int 1995; 56 (Suppl 1):S5-S7.
41. Rittweger J, Gunga HC, Felsenberg D, Kirsch KA. Muscle and bone - Aging and space. J Gravitational Physiol 1999; 6:P133-P136.
42. Schiano A, Elsinger J, Acquaviva PC. Les Algodystrophies. Armour-Montagu, Paris, 1976.
43. Schiessl H, Frost HM, Jee WSS. Perspectives: Estrogen and bone-muscle strength and "mass" relationships. Bone 1998; 22:1-6.
44. Schönau E, Frost HM. The "muscle strength-bone strength" relationship in humans. A review (A). In: Proceedings, Third International Congress on Osteoporosis. Xi'an, P.R. China, 1999:84-89.
45. Takahashi HE. Spinal Disorders in Growth and Aging (Ed) Springer-Verlag, Tokyo, 1995.
46. Takahashi HE. Mechanical Loading of Bones and Joints (Ed) Springer-Verlag, Tokyo, 1999.
47. Weinmann JP, Sicher H. Bone and Bones, 2nd Ed. CV Mosby Co, St Louis, 1955.
48. Woodard JC. Morphology of fracture nonunion and osteomyelitis. Vet Clin N Amer 1991; 21:813-844.

